

# CAREER: Enabling “White-Box” Autonomy in Medical Cyber-Physical Systems

Jin-Oh Hahn (PI, University of Maryland), Ali Tivay (PhD Student, University of Maryland)

Christopher G. Scully (Co-I, U.S. Food and Drug Administration)

## Interpretable Modeling of Cardiovascular Responses to Fluid Perturbation

### 1. Macroscopic View of the Circulatory System

- The circulatory nature of the cardio-vascular system is modeled as a loop.
- Through this loop, the heart pumps blood with rate  $Q$  (cardiac output).
- The resistance  $R$  (systemic vascular resistance) resists the flow of blood.
- Compartment fluid volumes determine mean arterial and venous pressures.
- Hemorrhage causes volume loss, while resuscitation causes volume expansion.

### 2. Fluid Shift ( $J_f$ ) Controller

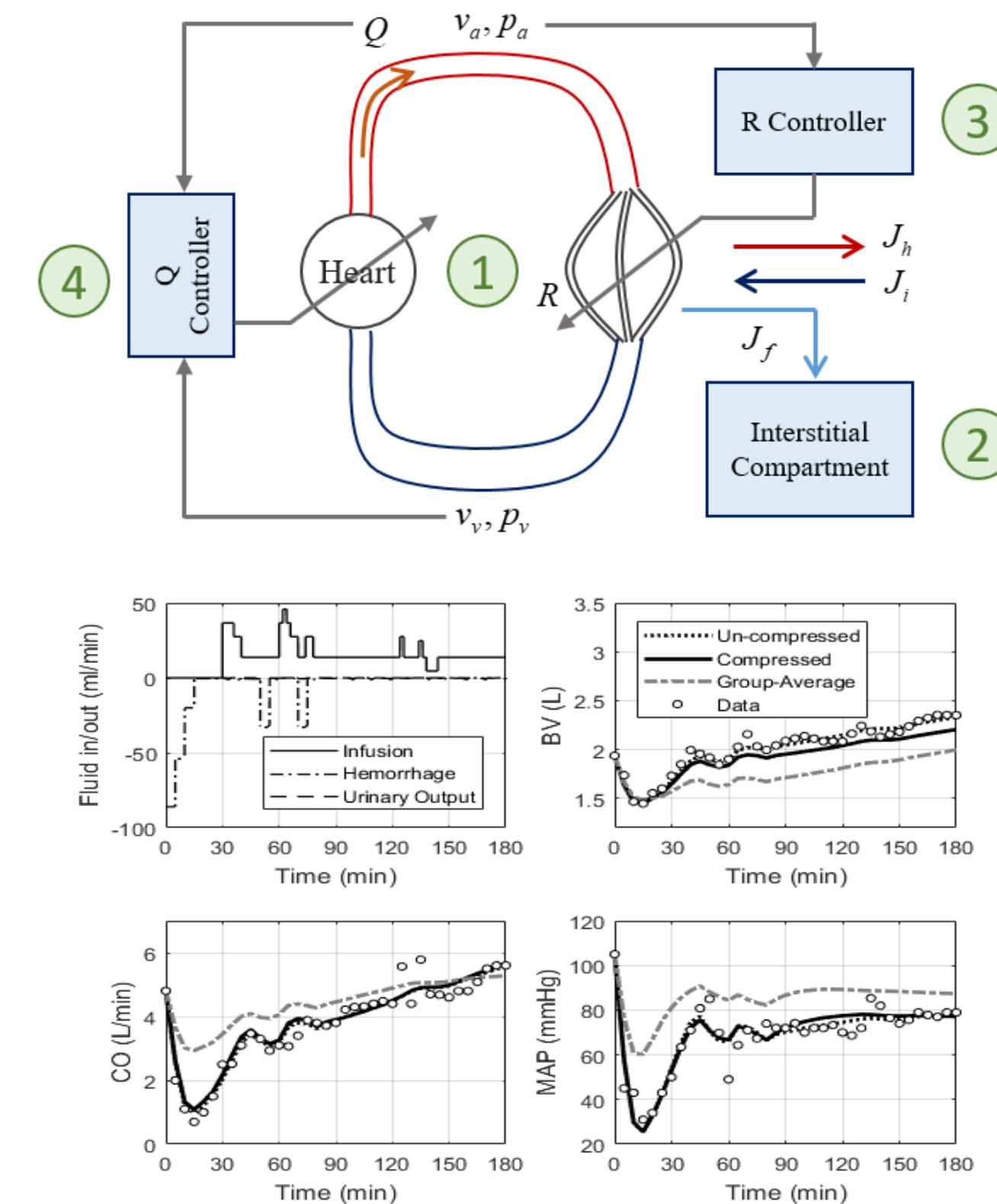
- Perturbation in blood volume is counteracted by an exchange of fluid with the interstitium.
- The net rate of fluid shift is modeled as a control input to regulate total blood volume.

### 3. Systemic Vascular Resistance ( $R$ ) Controller

- The body can change the resistance  $R$  through vasoconstriction and vasodilation.
- The resistance  $R$  is modeled as a control input that has the goal of regulating arterial pressure.
- This control input is also disturbed by changes in the fraction of red blood cells in the blood.

### 4. Cardiac Output ( $Q$ ) Controller

- The cardiac output  $Q$  is modeled as a controlled variable through heart rate and contractility.
- This controller is disturbed by changes in cardiac preload and loss of red blood cells.



## Data-Driven Generation of Virtual Patients using Physiological Models

### A. Variational Approach to Virtual Patient Generation

#### 1. Family of Distributions Over Latent Parameters $\phi$

- A distribution from the mean-field family is selected in the compressed latent space.
- Each dimension  $p_j(\phi_j)$  is characterized by a normal distribution.
- Parameters for  $p_j(\phi_j)$  are estimated from compressed calibration results in each latent dimension.

$$P(\phi) = \prod_{j=1}^{n_p} p_j(\phi_j)$$

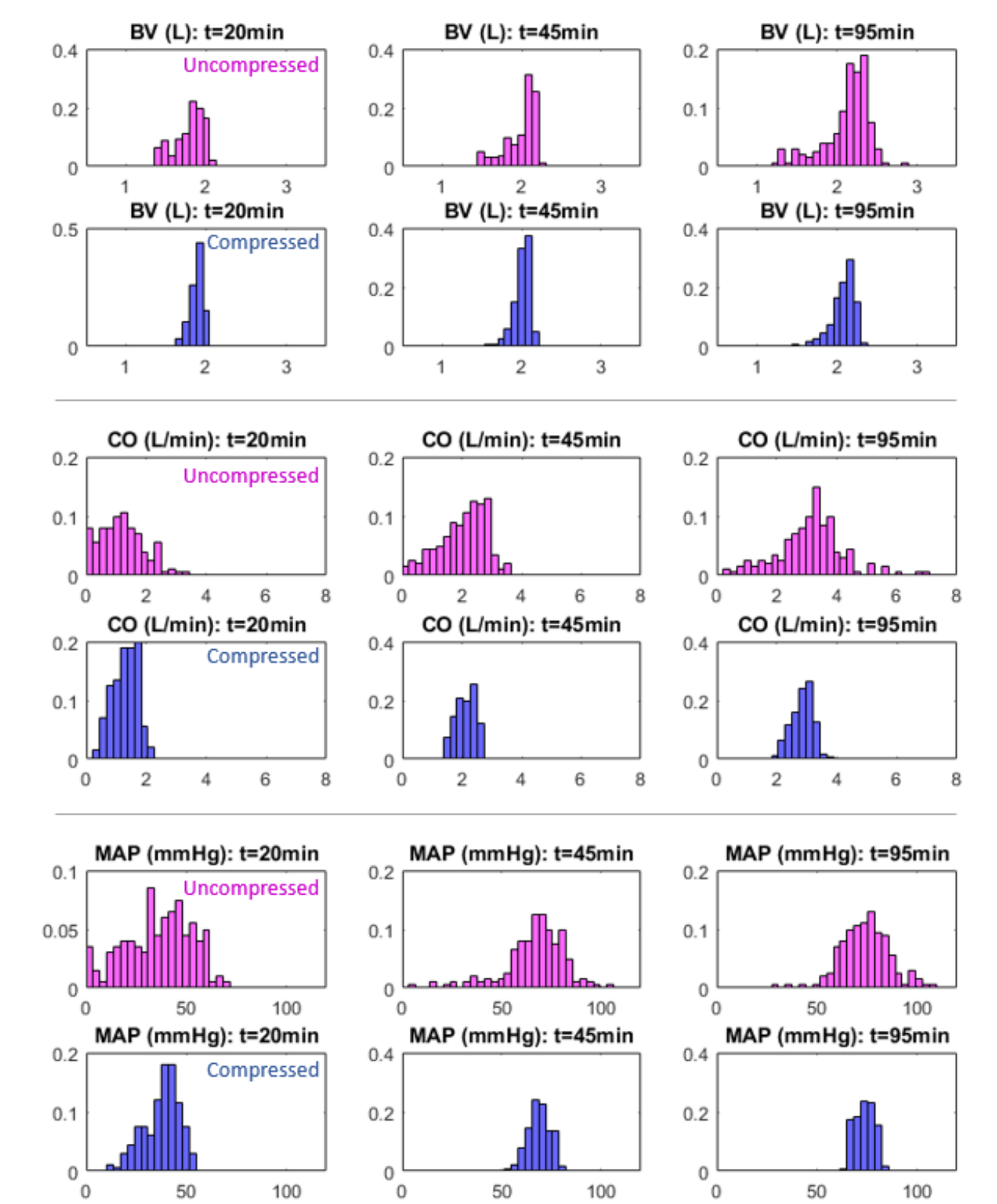
#### 2. Sample from $P(\phi)$ to Generate Virtual Patients

- Each sample  $\phi^{(i)}$  can be converted to model parameter  $\theta^{(i)}$  to simulate the virtual patient.

$$\theta^{(i)} = V\phi^{(i)} + \bar{\theta}$$

The results suggest that:

- Estimating  $P(\phi)$  *without compression* results in generation of *many* un-realistic virtual patients.
- Estimating  $P(\phi)$  *with compression* omits the un-realistic virtual patients.
- With compression, the range of observed variations in virtual patient behavior are more realistic.



## Compressed Patient-Specific Calibration of Physiological Models

### 1. Population-Average Model Calibration

- Diverse data from a population of subjects are used to calibrate the physiological model.
- The resulting model represents typical behavior in the population.

$$\bar{\theta} = \arg \min_{\theta} \left\| \mathbf{Y} - \hat{\mathbf{Y}}(\theta) \right\|_2^2$$

### 2. Compressed Patient-Specific Model Calibration

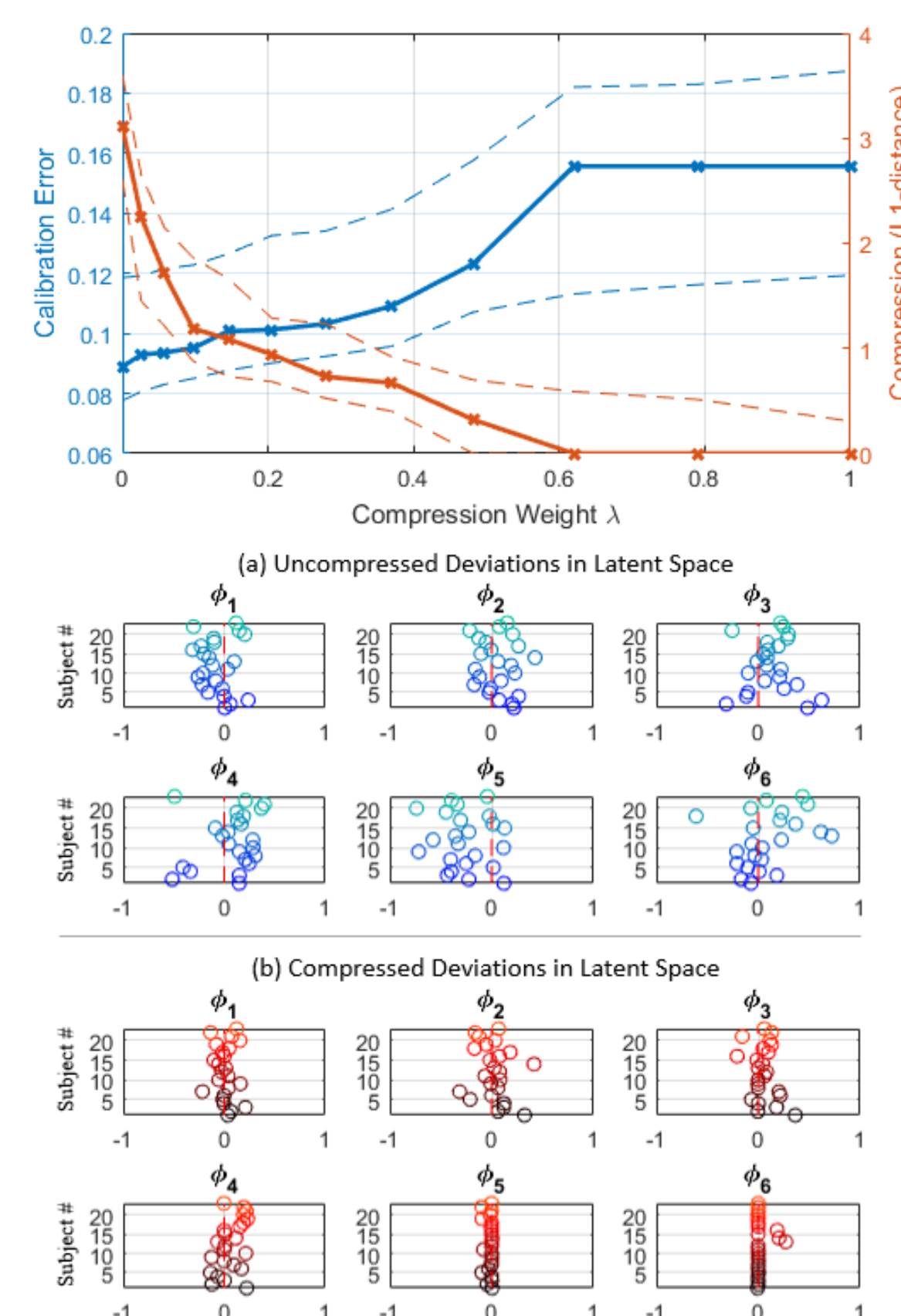
- Local parameter-output covariances ( $\mathbf{C}$ ) are computed around the population-average model.
- A singular value decomposition of  $\mathbf{C}$  gives the directions of maximum parameter-output covariance.
- The model can be calibrated to each subject in a compressed way as follows:

$$\mathbf{C} = \hat{\mathbf{Y}}_{\theta} \Theta^T = \mathbf{U} \mathbf{S} \mathbf{V}^T$$

$$\hat{\theta}_i = \arg \min_{\theta} \left\| \mathbf{Y}_i - \hat{\mathbf{Y}}(\theta) \right\|_2^2 + \lambda \left\| \phi \right\|, \quad \phi^T = (\theta - \bar{\theta})^T \mathbf{V}$$

The results suggest that:

- The model can be calibrated in a compressed way, to match the data from different patients.
- The variability across different subjects can be represented in the compressed latent space  $\phi$ .



### B. Markov-Chain Monte-Carlo (MCMC) Approach to Virtual Patient Generation

#### 1. The Virtual Patient Generation Problem

- To successfully use MCMC methods for virtual patient generation, two important elements must be designed:
- A *likelihood function*, that represents how likely it is for a proposed virtual patient to behave like a real subject from the dataset.
- A *prior distribution*, that encodes prior knowledge about “reasonable” parameter samples.

#### 2. The Likelihood Function

- $S$  is the set of real subjects in data, and  $S_i$  ( $i=1, \dots, m$ ) random subsets of  $S$  with size  $K$  ( $m$  is large).
- We accept a proposed virtual patient as likely if its behavior resembles any  $K$  patients in the dataset.

$$L(\theta) = \frac{1}{m} \sum_{i=1}^m \prod_{j \in S_i} P(\mathbf{Y}_j | \mathbf{I}_j, \theta)$$

#### 3. The Prior Distribution

- The regularizer used in compressed model calibration can be thought of as a Laplace prior.
- Thus, a Laplace prior (in latent space) is used, which is centered at the population average model.

The results suggest that:

- MCMC generates virtual patients that behave realistically and cover the range of observed behavior.
- The MCMC-sampled parameter values lie within their reasonable physiological ranges.

